Comparison of the Effectiveness of Four Different Crosslinking Agents with Hyaluronic Acid Hydrogel Films for Tissue-Culture Applications

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Received 23 October 2006; accepted 13 December 2006 DOI 10.1002/app.25993

Published online 5 March 2007 in Wiley InterScience (www.interscience.wiley.com).

ABSTRACT: The effectiveness of four different reagents, glutaraldehyde (GTA), 1-ethyl-3-(3-dimethylaminopropyl) carbodiimide (EDC), poly(ethyelene glycol) diglycidyl ether (EX 810), and divinyl sulfone (DVS) as crosslinkers for cast hyaluronic acid (HA) films has been evaluated. Films were prepared by casting from solution and exposed to solutions of the crosslinkers in acetone—water solution. Swelling in water and in phosphate buffered saline (PBS) was then used to assess the effectiveness of the crosslinkers. GTA-crosslinked films were found to be of low stability compared with those treated with EDC, EX 810, and DVS. Results suggest that instability in GTA-crosslinked materials arises in part from residual acid catalyst. The effects of polymer molecular weight are not uniform.

With GTA-crosslinked film produced from higher molecular weight HA swells more, and this is attributed to reduced diffusion of the crosslinker, but with EDC, the opposite effect is observed, implying some additional molecular weight dependent mechanism. Differential scanning calorimetry and dynamic mechanical thermal analysis results suggest that there are no significant structural difference between the gels for each crosslinker system and only the crosslink density and moisture content alters the transitions. © 2007 Wiley Periodicals, Inc. J Appl Polym Sci 104: 3183–3191, 2007

Key words: hydrogel; biological applications of polymers; biomaterials; mechanical properties

INTRODUCTION

Hyaluronan, also known as hyaluronic acid (HA), an abundant nonsulfated glycosaminoglycan (GAG) component of synovial fluid and extracellular matrices, ^{1,2} is an attractive building block for new biocompatible and biodegradable polymers with possible applications in drug delivery, ³ tissue engineering, ⁴⁻⁶ and visco supplementation. ⁷ As a polysaccharide of the extra cellular matrix (ECM), it plays a multitask role, having many structural, rheological, physiological, and biological functions in the body. It is a linear and anionic polymer consisting of two modified sugars, glucuronic acid and *N*-acetylglucosamine, with the molecular structure:-[D-glucuronic acid (1-b-3) *N*-acetyl-D-glucosamine (1-b-4)]_n.

Hyaluronan is synthesized by many types of cells in the body and extruded into the extracellular space where it interacts with the other constituents of the ECM to create the supportive and protective structure around the cells. It is present as a constituent in all body fluids and tissues and is found in higher concentrations in the vitreous humor of the eye and

the synovial fluid in the joints. Commercial HA is usually obtained from rooster comb, although full details of its preparation are not always provided.

The biomedical application of HA is hindered by its short residence time and lack of mechanical integrity in an aqueous environment and these drawbacks must be addressed in order to realize its potential. In this article, we compare the effects of four different chemical crosslinkers to protract the material's degradation and dissolution and thereby improve mechanical stability. Crosslinking is the most common modification of hyaluronan to form a hydrogel and a number of mechanisms have been reported in the literature.8-11 The functional groups, which are mainly responsible for crosslinking of HA molecules are the hydroxyl and carboxyl groups. Hydroxyl groups may be crosslinked via an ether linkage and carboxyl groups via an ester linkage. If desired, the HA may be chemically modified prior to crosslinking to form other chemically reactive groups. Thus, for example, HA may be treated with acid or base such that it will undergo at least partial deacetalization, resulting in the presence of free amino groups. It is said that amino groups may be crosslinked via an amide (-C(O)-NH-); imino (-N=CH-) or secondary amine (-NH-CH-) bond. An imino linkage can be converted into an amine linkage in the presence of a reducing agent.

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Journal of Applied Polymer Science, Vol. 104, 3183–3191 (2007) © 2007 Wiley Periodicals, Inc.



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Scheme 1 With water soluble carbodimides (WSC) (2) the crosslinking occurs through the initial formation of O-acylisourea (3) on the polysaccharide, through reaction with neighboring carboxyl groups (1) an anhydride (4) is formed, and this anhydride then reacts with nearby hydroxyls to give both inter- and intramolecular crosslinks.

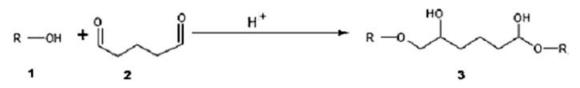
Reaction has been accomplished under acidic, neutral, and alkaline conditions using carbodimides, ^{10,12–14} hydrazides, ^{14,15} aldehydes, ⁸ sulfides, ¹⁶ and polyfunctional epoxides. ^{9,17–20} Autocrosslinking ^{21,22} and photocrosslinking ^{23–25} have also been reported. With carbodimides, the crosslinking occurs through the initial formation of anhydride on the polysaccharide, through reaction with neighboring carboxyl groups, and this anhydride then reacts with nearby hydroxyls to give both inter- and intramolecular crosslinks. It was postulated that crosslinking took place via ester groups. Scheme 1 gives some details of these reactions. A reported 10 modification of this reaction introduces L-lysine methyl ester, which offers the opportunity to form higher stability amide crosslinks. Dialdehydes are believed to crosslink through formation of acetal or hemiacetal groups on neighboring chains, with kinetic and spectroscopic evidence indicating a prevalence of the hemiacetal. Glutaraldehyde (GTA) is believed to form either a hemiacetal or an ether link with HA under acidic conditions²⁶ as shown in Scheme 2. With divinyl sulfone (DVS), the crosslinking occurs via the hydroxyl groups forming an ether bond as shown in Scheme 3. The epoxy group of EX 810 is known to react with -COOH and the —OH functional groups, therefore forming ester and ether bonds, respectively, and is shown in Scheme 4.

Reactions may be carried out using heterogeneous or homogeneous methods. Heterogeneous reactions are carried out on solid HA, cast in the form of films or membranes, in which case diffusion rates maybe at least as important as chemical kinetics, whereas homogeneous reactions are carried out using HA solutions. The former method has the advantage of allowing shaping of a product before crosslinking, whereas the latter method offers the advantage of better control of the chemistry with greater product homogeneity.

Experience has shown that the repeatability of reported experimental procedures and their outcomes is low, perhaps because of differences in the sources and preparation procedures of the HA and the HA solutions. Therefore, an important consideration in the work reported here was to compare, under a set of standard conditions, the performance of four important crosslinkers using well characterized HA from identified sources.

The first part of the study established a method for the controlled dissolution of HA and film casting, and then utilized the crosslinking reagents to give materials with increased stability with time. Control of dissolution procedure is considered to be important because dissolution and solution degradation may be concurrent processes. Complete dissolution is also important to maximize intermolecular crosslinking and reduce wasteful intramolecular reactions. Previously, crosslinking HA films by immersion in a crosslinking mixture has only been reported for GTA⁸ and carbodiimide.¹⁰

The relationship between crosslink density and solvent swelling is described by the well-known Flory–Rhener equation, which demonstrates that increasing crosslinker effectiveness will be shown by a reduced volumetric swelling. For this work,



Scheme 2 The OH (1) group on the hyaluronic acid reacts under acidic conditions with glutaraldehyde (2) to give hemiacetal or ether crosslinks (3).

Scheme 3 The OH (1) group on the hyaluronic acid reacts under alkaline conditions with divinyl sulfone (2) to give sulfonyl bisethyl crosslinks (3).

the swelling ratio (SR) was calculated via the equation:

Swelling ratio =
$$\frac{W_s}{W_d}$$

where W_s is the weight of the sample at equilibrium at each temperature and W_d is the weight of the dried sample.

Huglin et al. defines the equilibrium water content according to the equation:

$$EWC = \frac{(SR - 1)}{SR}$$

Therefore, the water content can be expressed as follows²⁷;

$$W_b(\%) = W_t - (W_f + W_{fb}) = W_t - (Q_{\text{endo}}/Q_f) \times 100$$

where W_b is the amount of bound water (%); W_f and W_{fb} are the amounts of free and freezing bound water, respectively, and W_t is the EWC (%).

The three types of water found in gels are defined as follows:

1. Bound water: this term refers to the water molecules that are bound to polymer molecules through hydrogen bounds. This kind of water shows no endothermic peak in the temperature range: -70 to 0° C.

- 2. Intermediate water or "secondary bound water:" other water molecules that interact with polymer molecules are referred to as intermediate water. This kind of freezing water has a melting point <0°C.
- 3. Free water: water molecules that do not take part in hydrogen bonding with polymer molecules are called free water because of their greater degree of mobility in comparison with other water molecules. Free water is freezing water showing a melting point at 0°C. ²⁸

An initial set of survey experiments compared the effects of the different crosslinkers and reaction environments, and the results obtained were then used in designing the experiments to determine the reaction conditions for further experiments.

EXPERIMENTAL

Materials

The sodium salt of HA with an average molecular weight of 2.14×10^6 was supplied by Clear Solutions (New York, NY) as dry powder. This material is prepared in high yield from streptococcus bacteria by fermenting the bacteria under anaerobic conditions in CO_2 enriched growth medium.²⁹ HA powders of average molecular weight 1.2×10^6 , 8.5×10^5 , and 1.4×10^5 were purchased from Bioiberica (Barcelona, Spain). This material is obtained from rooster comb. HA has been mainly extracted from rooster combs for many years and many papers have been published on clinical application of HA from this source. 1-Ethyl-3-(3-dimethylaminopropyl) carbodiimide (EDC), GTA, poly(ethylene glycol) diglycidyl ether, and DVS were purchased from Lancaster (UK).

Preparation of HA-crosslinked films

Solutions were prepared by sieving HA particles into double-distilled water to expose the maximum

Scheme 4 The OH (1) group on the hyaluronic acid reacts with the epoxy group of the poly(ethyelene glycol) diglycidyl ether (2) to give ether crosslinks (3).

area for solvent interaction. This was followed by agitation, to minimize shear stress, in a shaking bath at 25°C for up to 102 h and was found to give reproducible solutions of uniform viscosity. The viscosity time profiles of the solutions were then obtained using an Ubbelohde viscometer. Samples were fully dissolved after 24 h and the molecular properties of all the solutions were evaluated using size exclusion chromatography (SEC). Films were then prepared by casting a 1 wt % aqueous solution of each HA type onto a clean petri dish, followed by drying at 25°C under vacuum for 120 h. The volume of solution used determined the thickness of the resulting film and this was adjusted to give a thickness of ~ 0.2 mm.

For the initial survey experiments, $10 \times 10 \times 0.2$ mm³ samples of cast HA ($M_W = 7.6 \times 10^5$ Da) film were weighed and placed in 10 mL of acetone-water solution (80:20 by volume) containing 0.01M HCl and varying mole ratios of 1-EDC, GTA, ethylene glycol diglycidyl ether (Denacol EX-810), and divinylsulphone (DVS). The acetone prevents the dissolution of the HA film into the reaction solution, and all the reaction vessels were sealed to prevent evaporation of the acetone. The acetone concentration of 80 vol % was selected after experimentation had shown that lower concentrations resulted in excessive water swelling of the cast HA film. Crosslinker molarity and mole ratio of crosslinker to HA were based on previously published data.8 A high crosslinker concentration is used to drive the diffusion process. The crosslinking reaction was allowed to proceed at room temperature for 24 h unless otherwise specified. With EDC and GTA, crosslinking is favored by acidic conditions and 0.01M HCl was used as pH adjuster and catalyst,8 while DVS requires alkaline conditions and in this case, 0.01M NaOH was used to adjust pH.

Characterization of films

On the basis of the initial observations, further series of crosslinked films were cast, using film thicknesses up to 0.2 mm, crosslinking times between 24 and 72 h, and crosslinking temperatures of 4 and 20°C. The crosslinker:HA mole ratio used was 2:1 to 4:1 and the medium was 80:20 acetone:water. These films were washed in distilled water for 1 h and then dried overnight in a vacuum oven at room temperature. They were then swollen in distilled water and in phosphate buffered saline (PBS) and the water content of the gel and the SR were measured.

DSC analysis was carried out on a TA Instruments DSC 10 differential scanning calorimeter. The thermal analysis profiles were of dried hydrogel samples and swollen samples. The temperature was increased from room temperature to 300° C at a rate of 10° C/min under a nitrogen atmosphere. Differential

scanning calorimetry (DSC) (TA Instruments 10) was also employed to examine the state of water in the swollen hydrogels with different water contents. Samples sealed in aluminum pans were cooled to −20°C and then heated to 20°C at a heating rate of 5°C/min under 60 cc/min of nitrogen gas flow. Using peak areas, normalized for sample mass, the endotherm associated with water loss was obtained and compared with the theoretical value for water. The fraction of free water in the total water was then calculated using eq. (3) as the ratio of the endothermic peak area for water-swollen hydrogels to the melting endothermic heat of fusion (-334 J/g) for pure water. Bound water because of hydrogen bonding was expressed as the difference between the total water and the free water.

The dynamic mechanical thermal analysis (DMTA) of the materials in the form of films (0.7-mm thick) was carried out with a Polymer Laboratories DMTA MK-1 apparatus, operating in the parallel plate mode. The scans were performed on samples maintained under room conditions, at a frequency of 1 Hz, temperature range of -30 to 100°C, and a heating rate of 4°C min⁻¹.

RESULTS AND DISCUSSION

Preparation of HA films

The relative flow times for the HA solutions (Fig. 1) are consistent with the molecular weights indicated by the suppliers. All the viscosity-time curves have a similar shape with the samples becoming fully solvated between 24 and 40 h. After this time, the solution viscosities are seen to fall and this is taken to indicate the onset of polymer degradation through hydrolysis. As a result of these observations, all films used for crosslinking were cast after 24 h of dissolution and thus in the fully solvated and chain-disentangled state. The molecular properties of each

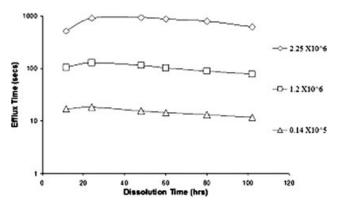


Figure 1 Dissolution time profile of 1 wt % hyaluronic acid (HA) solutions.

Intrinsic Radius of Radius of Mark-Houwink Mark-Houwink viscosity hydration gyration Sample M_w/M_n (dL/g)(nm) (nm) (α) (log K) -2.49 2.25×10^{6} 1.08 24.61 94.84 162.61 0.61 1.20×10^{6} 2.14 20.13 66.54 114.33 0.91 -4.23 0.85×10^{6} 3.27 14.80 51.68 97.01 0.95 -4.44 0.14×10^{6} -9.8841.38 3.26 18.31 26.94 1.09

TABLE I Molecular Properties of Hyaluronic Acid After 24 h Dissolution, Measurements were in PBS

sample is summarized in Table I and the values given were calculated using the Viscotek Omnisec software, version 4.2.

Table II summarizes the results of the survey experiments and details the swelling ratios of the films after they had been submerged in the solution of crosslinker in 80% acetone and 20% water for 24 h. The results show that the molarity of the crosslinker solution has only small effect indicating that film surface area is the critical issue. With both DVS and GTA, the need for acidification to optimize crosslinking is apparent.

Swelling studies

In Figures 2 and 3, the swelling in water and PBS of films, crosslinked under optimum conditions, is compared and in both media all three crosslinkers give an initial volume swelling of between 2.0 and 2.5, indicating similar crosslink densities. Considering the behavior in distilled water, both the DVS

and EDC-crosslinked materials shrink with time and this is taken to indicate continuing crosslinking action, suggesting that the crosslinker diffusion into the film is faster than the crosslinker reaction with the constituent polymer.

GTA-crosslinked materials are clearly very sensitive to the nature of the swelling medium and it is thought that the lower swelling and greater stability in buffer arises from neutralization of residual acid in the film. With these materials, progressive swelling occurs in water and this is thought to arise from network scission. On the basis of Tomihata and Ikada's proposal that the crosslinks in this case are hemiacetals,⁸ as shown in Scheme 2, it is reasonable to presume that these are undergoing hydrolyitic scission with time, catalyzed by residual acidity, and then the gel SR increases as the crosslink density falls. Taken overall, these results suggest that the crosslinking reagents remain reactive in the gel and that swelling with buffer has a stabilizing effect through neutralization.

TABLE II Crosslinking Conditions for HA Films (\sim 0.1-mm Thick) $M_w = 8.5 \times 10^5$ Da

Crosslinker	Mole Ratio crosslinker/polymer	[crosslinker] M	рН	Equilibrium swelling ratio after 24 h in 80% acetone/20% water mixtures
DVS	02:01	0.26	12	1.53
DVS	04:01	0.57	12	1.37
GTA	02:01	0.19	2	1.28
GTA	02:01	0.19	2	1.28
GTA	02:01	0.21	2	1.27
GTA	02:01	0.22	2	1.26
GTA	02:01	0.22	2	1.26
GTA	04:01	0.40	2	1.20
EDC	01:01	0.14	2	1.67
EDC	02:01	0.22	2	1.47
EDC	02:01	0.30	2	1.33
EDC	03:01	0.26	2	1.57
EDC	04:01	0.46	2	1.28
EDC	04:01	0.46	2	1.28
EDC	04:01	0.58	2	1.31
EX 810	04:01	0.28	2	1.17
EX 810	04:01	0.32	2	1.25
EX 810	04:01	0.34	2	1.21
EX 810	04:01	0.36	2	1.21
EX 810	02:01	0.17	7	1.33
EX 810	02:01	0.22	7	1.20

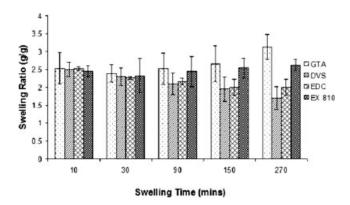


Figure 2 Swelling ratios in distilled water at 22°C (hyaluronic acid (M_w 0.14 × 10⁶ Da) to crosslinker is 1 : 5 for all samples).

Degradation of films

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Figures 4–6 show the results of longer time scale swelling experiments with HA of different initial molecular weights. HA molecular weight can be expected to influence gel character in two ways. Diffusion of reactants can be expected to occur faster in lower molecular weight polymer because of increased chain end free volume, thereby increasing crosslink density, but counteracting this will be the more rapid macronetwork formation with higher molecular weight chains. With the lower molecular weight HA, the gels reached their maximum SR at 24 h and after this time start to degrade, presumably through both crosslink hydrolysis and main-chain scission. At 5 days, water contents reach 98% and gels started to break up.

The two crosslinkers EDC and GTA were chosen for further swelling experiments at 37°C on thicker films (0.2 mm). Figures 7 and 8 show the swelling characteristics of films produced by EDC and GTA crosslinking, respectively, and the time scale of over 3 weeks demonstrates their long term stability. As expected, the SR decreases slightly with increased

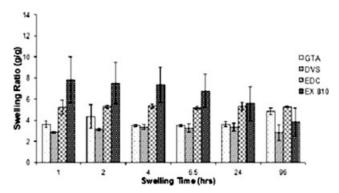


Figure 4 Crosslinked hyaluronic acid films (M_w 2.25 \times 10⁶ Da) swollen in distilled water pH 6.2 at 25°C, monomer crosslinker mole ratio 1 : 4.

crosslinker mole ratio, reflecting the consequent increase in crosslink density; however, this effect is small confirming that the surface area is the dominating factor. When compared with the GTA-crosslinked materials, EDC-crosslinked films seem to be more stable and the degradation appears to occur via the main chain as opposed to crosslink scission. However, the GTA-crosslinked films show a large initial increase in volume before a reduction in swelling occurs and it is possible that this initial swelling is due to crosslink scission and the consecutive reduction in swelling can be attributed to main-chain degradation. This behavior is consistent with the presumed mode of crosslinking of these reagents, as shown in Schemes 1 and 2, in that hemiacetal crosslinks, obtained by reaction with GTA, can be expected to be of low stability compared with the anhydride derived crosslinks arising with EDC. It is likely that the small increase in SR apparent in Figure 4 with the GTA-crosslinked material reflects the early stages of network breakdown. With both GTA and EDC crosslinker, molarity has the expected small effect, again indicating that surface area is the dominating factor.

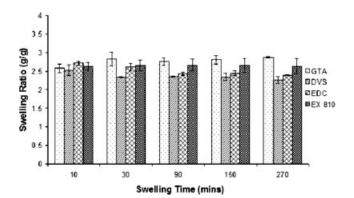


Figure 3 Swelling ratios in PBS at 22°C (hyaluronic acid $(M_w 0.14 \times 10^6 \text{ Da})$ to crosslinker is 1 : 5 for all samples).

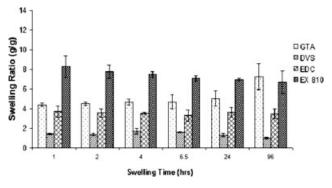


Figure 5 Crosslinked hyaluronic acid films (M_w 1.20 \times 10⁶ Da) swollen in distilled water pH 6.2 at 25°C, monomer crosslinker mole ratio 1 : 4.

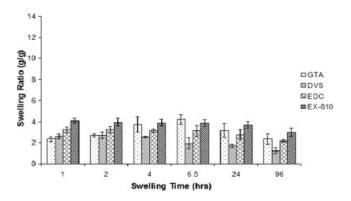


Figure 6 Crosslinked hyaluronic acid films (M_w 0.14 \times 10⁶ Da) swollen in distilled water pH 6.2 at 25°C, monomer crosslinker mole ratio 1 : 4.



The thermal behavior of the HA-hydrogel film was investigated by DSC analysis (Figs. 9 and 10). All the samples showed the presence of a broad endothermic peak below 85°C (Table III) and this is thought to be associated with the loss of moisture remaining after the drying procedure. In addition, significant sharp exothermic peaks were observed for each sample, which probably represent decomposition. The DSC profiles show that after HA was crosslinked, the endothermic and exothermic peaks shifted, indicating an altered structure. The relatively low endotherm peak temperature obtained with the EDC-crosslinked material may reflect lower water retention through the drying period.

Figure 10 shows the DSC thermograms of the fully swollen hydrogels. The endothermic peak maximum of the swollen hydrogel ranges between -1.17 and 2.5° C. The fraction of free water in total water is approximately calculated as the ratio of the endothermic peak area for water-swollen hydrogel to melting endothermic heat of fusion (-334 J/g) for

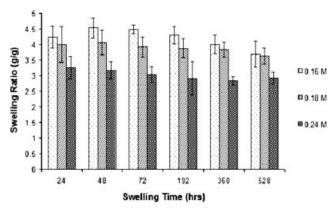


Figure 8 Swelling of HA films (8.5×10^5 Da) in distilled water at 37° C when crosslinked with EDC.

pure water as described in Mansor and Malcolm's work.³⁰ The bound water is expressed as the difference between the total and free waters. The EWC value and the free and bound water contents were calculated and are listed in Table IV. The EWC was calculated at pH 7 in water at 25°C. Clearly, samples with the highest crosslink density have the lowest EWC and free water content indicating a more compact structure.

The dynamic mechanical analysis results shown in Figure 11 indicate that there is little change in the storage modulus between the initial temperature and 15° C. However, between 20 and 40° C, the storage modulus drops by over two orders of magnitude. This abrupt change in physical properties is associated with the onset of short-range molecular motions at the glass transition. Because of the crosslinking, the modulus beyond the glass transition does not decline to near zero and the materials still exhibit useful load bearing characteristics even $50-75^{\circ}$ C above T_g . The logarithmic plot shows that, for HA crosslinked systems, a direct relationship is found between post- T_g modulus and the degree of

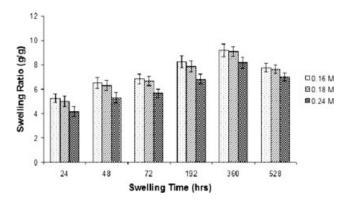


Figure 7 Swelling of HA films $(8.5 \times 10^5 \text{ Da})$ in distilled water at 37°C when crosslinked with GTA.

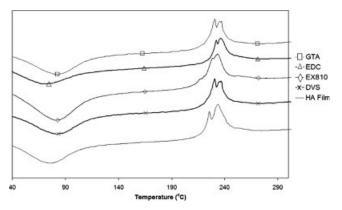


Figure 9 The thermal behavior of HA films crosslinked and uncrosslinked prior to swelling.

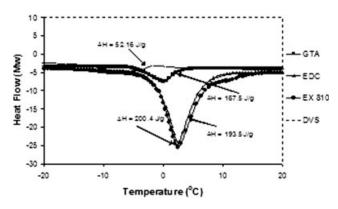


Figure 10 Crosslink density effect on the endotherm.

crosslinking, i.e., the EDC-crosslinked HA had lowest crosslink density and therefore the lowest post T_g modulus. Interestingly, the GTA-modified samples seem to soften at a lower temperature than the rest of the films and this may explain their high swelling ratios at room temperature (Fig. 2).

At low temperatures, leading up to the glass transition, $\tan \delta$ is well below 0.1 (Fig. 12). The rapid rise in the $\tan \delta$ curve coincides with the rapid decline in the storage modulus confirming that this is the glass transition. For all the HA-crosslinked systems, the $\tan \delta$ values above T_g are relatively low. Interestingly, sharp peaks are observed for the highly swollen samples. The magnitude and broadness of the peak seem to be related to changes in the degree of swelling. GTA-crosslinked materials had a broadest peak and a SR of 3.5 while the sharpest peak was obtained with the highest SR of 13.3 for EDC-crosslinked materials. EX 810 crosslinked materials and DVS crosslinked materials had swelling ratios of 7.7 and 6.5, respectively.

For clarity purposes, a linear scale was used for all storage modulus data, however there was no occurrence of secondary thermal transitions in the films and no inflections or peaks were noticed, confirms that the structure of the films is similar.

TABLE III
DSC Data for Unmodified and Modified Hyaluronic Acid
Films Prior to Swelling

	Endothermic	Degradation temperature (°C)		
Sample	peak (°C)	First peak	Second peak	
HA unmodified	76.1	233.3	234.3	
EDC	74.9	232.2	236.8	
DVS	83.1	231.1	236.5	
EX810	83.6	229.9	234.4	
GTA	83.1	231.0	236.1	

TABLE IV Water Content of the Gels Used in the Degradation Study (Fig. 6)

Sample	EWC (%)	Bound water W_b (%)	$W_f + W_{fb}$ (%)
EDC	81.2	23.27	57.93
DVS	70.2	15.61	54.57
EX810	82.0	22.04	60.00
GTA	70.9	20.79	50.14

All samples were swollen at pH 6.2 in water at 25°C.

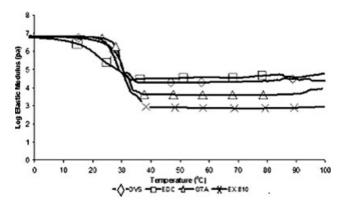


Figure 11 Storage modulus versus temperature of swollen hyaluronic acid films.

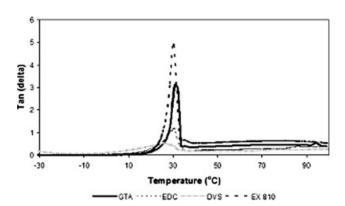


Figure 12 Tan δ versus temperature of highly swollen hyaluronic acid films. The T_g is similar for all samples.

CONCLUSIONS

When HA is cast in a fully solvated and chain-disentangled state, films can be crosslinked with GTA, 1-EDC, poly(ethyelene glycol) diglycidyl ether (EX 810), and DVS by immersion in solutions of the crosslinker in 80% acetone–water mixtures. Swelling studies showed that both the molecular weight of the films and the crosslinker type influenced the crosslink density of the films. Diffusion of the crosslinker through the films played a significant role. GTA-crosslinked films were found to be of low stability compared with those treated with EDC, EX 810, and DVS. Results suggest that instability in GTA-crosslinked materials arises in part from residual acid catalyst. When compared with the GTA-

crosslinked materials, EDC-crosslinked films seem to be more stable and the degradation appears to occur via the main chain as oppose to crosslink scission. The GTA-crosslinked films show a large initial increase in volume before a reduction in swelling occurs and it is possible that this initial swelling is due to crosslink scission and the following reduction in swelling can be attributed to main-chain degradation. The effects of polymer molecular weight are not uniform. The thermal and structural properties of the films were further studied by DSC and DMTA and it was found that films were structurally similar and had almost identical thermal behavior. The main difference in the films appears to be due to crosslink density variations.

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